

ANALYTICAL METHOD COMPRISING ADDITION IN TWO OR MORE
POSITIONS AND A DEVICE AND TEST KIT THEREFOR

Technical field

5 The invention relates to a method for determination of an analyte in a sample by use of biospecific affinity reactants (Reactant 1, Reactant 2 etc.), one of which is analytically detectable (Reactant*) and one is firmly anchored in a detection zone in a transport flow matrix
10 (Reactant I). The sample (analyte) is transported by a flow in the matrix from one application zone for liquid (LZS) containing the analyte (sample) and/or a buffer, to the detection zone (DZ), in which Reactant I is firmly anchored. At the same time as the sample is transported in
15 the matrix the soluble reactants, including Reactant*, are also being transported. In the detection zone Reactant* is captured in an amount which is related to the amount of analyte present in the sample. To achieve this, Reactant* is chosen so that it may bind biospecifically directly to
20 Reactant I or indirectly via one or more added biospecific affinity reactants (including the analyte). The amount of analyte is then determined from the amount of Reactant* bound in the detection zone. The transport flow may contain zones, in which different biospecific affinity reactants
25 (e.g. Reactant*, but not analyte) have been applied in advance (predeposited) in order to be dissolved and transported along with the flow towards the detection zone.

By reactants (including the analyte), exhibiting
30 biospecific affinity (bioaffinity reactants), are meant individual members in the reactant pairs: antigen/hapten - antibody; biotin - avidin/streptavidin; two complementary single chains of nucleic acid etc. As antibodies antigen binding antibody fragments such as Fab, F(ab)₂, single
35 chain Fv antibodies (scFv) etc. are considered. Relevant reactants do not have to be naturally occurring but can also be synthetically produced molecules/binders.

The type of test methodology in question has previously been used primarily for biospecific affinity reactants where at least one part of an employed reactant pair has exhibited protein structure, in particular in connection with so called immunochemical determination processes.

The biospecific affinity reactions are primarily performed in aqueous media (e.g. water).

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The technique in question is well known and has often been applied to so called test strips, where the strip has functioned as a flow matrix. The flow has been initiated in the zone to which the sample has been added (LZS). The flow has often been lateral, i.e. parallel to the surface of the matrix, or of other types, e.g. in depth in the matrix.

The test protocols have been of so called inhibition type (competitive) or non-inhibition type (non-competitive, sandwich). See e.g. Behringwerke US 4,861,711; Unilever WO 88/08534; Abbot US 5,120,643; Becton Dickinson EP 284,232 and US 4,855,240; Abbot/Syntex US 4,740,468; Pharmacia AB, WO 96/22532, etc.

In this context one often mentions simultaneous and sequential methods (protocols) regarding certain reactants (especially analyte and Reactant*). In simultaneous variants analyte (sample) and the relevant reactant, e.g. Reactant*, are transported simultaneously into the detection zone. Simultaneous variants may be obtained, if a sample is pre-incubated/mixed with Reactant* or if Reactant* has been predeposited in the sample application zone or in a zone downstream of the sample application zone but before the detection zone. In sequential variants the analyte (sample) is transported before a reactant, e.g. Reactant*, into the detection zone. Sequential variants may be obtained, if the relevant reactant, e.g. Reactant*, is added to the same application zone as the sample after the

sample (analyte) has been transported out of the zone. A variant of sequential methodology is discussed in US 4,855,240 (Becton & Dickinson). As an alternative to the sample (analyte) being transported before "tracer"

5 (=Reactant*) in the same transport flow, US 4,855,240 describes separated transport flows, in which the time of transport is regulated such that sample (analyte) reaches the detection zone before the "tracer" (Reactant*).

10 The term simultaneous tests has often included every variant, in which sample and Reactant* are pre-incubated/mixed before being added to a flow matrix or in which sample is added to a flow matrix, in which Reactant* is predeposited in the sample application zone or
15 downstream thereof. The term sequential tests has similarly included every variant, in which Reactant* is added to the sample application zone after the sample has migrated out of its application zone. Thus, considerations have not been taken, concerning if the order of analyte and Reactant* is
20 changed during transport to the detection zone. If not otherwise stated, this nomenclature is also used for the present invention, but is now adapted so that there are several application zones for liquid. This view means that primarily the initial order is considered, when both
25 analyte and Reactant* are in soluble form, and not the order in which analyte and Reactant* are transported into the detection zone.

Disadvantages with prior art and objects of the invention.

30 The prior art has often involved practical problems on automation, primarily because pre-incubation or sequential addition of sample and reactants have often been required, often in a certain predetermined order defined by the test protocol used. The object of the invention is to (a)
35 facilitate automation, (b) avoid sequential addition of sample and the analytically detectable reactant (Reactant*), and (c) allow for pre-deposited Reactant* when using sequential methodology, which relates to analyte and

Reactant*. More general aims are to achieve high quality test results, preferably with improved sensitivity and precision than given by previous variants.

5 The invention

Surprisingly we have now discovered that if flow is initiated by almost simultaneous addition of liquid to two adjacent zones in a flow matrix, the liquid added in the downstream zone migrates before the liquid which has been added in the upstream zone in direction towards the detection zone. Our discovery involves that zonewise migration of liquids may also be obtained if addition of liquid in an upstream zone is performed after addition of liquid in the nearest downstream zone. By applying this discovery on the relevant type of analysis methods, improvements can be obtained regarding the objects stated above.

A first main aspect of the invention relates to the initially mentioned analysis methods and is characterized in that

A. the flow matrix exhibits at least two application zones for liquid arranged substantially adjacent to each other:

25

$LZ_m \quad . \quad . \quad . \quad LZ_n \quad . \quad . \quad . \quad LZ_1 \quad . \quad . \quad . \quad DZ$
 ----->

wherein

30 a) LZ_n is an application zone for liquid, where n is the position of the application zone LZ_n ; (n is an

integer $2 < n \leq m$)

Removed:
New matter

b) m is the total number of application zones, in which flow is initiated,

35 c) one LZ_n is an application zone for sample (LZ_n, S) and one $LZ_{n'}$ is application zone for Reactant*

($LZ_{n'}, R^*$) with $n' \geq n$,

- B1
- d) -----> is the direction of the flow, and
e) DZ is detection zone, and

B. flow is initiated by adding liquid to each zone

- 5 $LZ_m . . . LZ_n . . . LZ_1$ in such a way that liquid_{n+1}, added to the application zone LZ_{n+1} , is transported through the matrix after liquid_n, added to the nearest downstream application zone LZ_n .
- 10 Liquid_{n+1} may easily migrate immediately after liquid_n, if the corresponding zones for application of liquid are adjacent to each other or if added liquid volumes are adapted for this aim.
- 15 In the most common case the above mentioned involves adding liquid_{n+1} to LZ_{n+1} before or primarily simultaneously with adding liquid_n to LZ_n . For $n = m$, LZ_{n+1} is lacking, and for that zone it is therefore not possible to add any liquid to LZ_{m+1} . Practical advantages are achieved if the addition is
- 20 performed primarily simultaneously for all $LZ_m . . . LZ_n . . . LZ_1$.

The number (m) of application zones for liquid ($LZ_m . . . LZ_n . . . LZ_1$) may in principle be any number with

25 the exception of one ($m \neq 1$). For practical reasons it is likely that in the future $2 \leq m \leq 10$, preferably $2 \leq m \leq 6$, such as $m = 2$ or 3 or 4 or 5.

- The liquids added (liquid₁ . . . liquid_m) may consist of
- 30 only buffer solution or buffer solution plus a reactant (Reactant 1, Reactant 2 etc.), needed to make it possible for Reactant* to be captured in the detection zone in an amount related to the amount of analyte in the sample. Also Reactant* may be included in a liquid_n. As a rule the
- 35 composition of transported components from an application zone is not the same as from the nearest adjacent application zone, in which flow is initiated (LZ_{n+1} and LZ_{n-1}

with the exception of $n = m$ and $n = 1$ for which the zones LZ_{n+1} and LZ_{n-1} , respectively, are lacking).

By the expression "substantially adjacent to each other" is meant that the application zones for liquid are immediately adjacent to each other or with an intermediate area of matrix which preferably is no more than about 2 mm, and particularly no more than about 1 mm.

10 A liquid added in an application zone may have a tendency to spread on top of the matrix to parts of the matrix being outside the zone. For adjacent zones this means that liquids may be mixed with each other in an undesired way. To avoid this, physical barriers delimiting two adjacent application zones (zone spacers) are placed. The barriers should primarily be placed on top of the matrix, but may be extended down into the matrix without completely quenching the flow. Delimitation is primarily against an adjacent zone for application of liquid, but can of course extend around a whole application zone for liquid. Liquid may also be introduced via pads or material layers applied on the matrix and from the same or a different material than the matrix material. In such as case there is no need for zone spacers.

25 Relevant reactants may be predeposited in an application zone for liquid (LZ_n) or between two such zones. An application zone for liquid, only intended for transporting buffering components and/or other components not participating in the biospecific affinity reactions (i.e. liquid neither containing nor intended for transport of any reactant or analyte), is called LZ_nB below. An application zone for liquid (LZ_n), where the liquid contains a reactant or is intended for transport of a reactant, e.g. Reactant*, Reactant 1, Reactant 2 etc., is called $LZ_n...R^*$, $LZ_n...R1$, $LZ_n...R2$ etc. below. If a liquid_n is to transport a combination of components, e.g. Reactant* and analyte (sample) the application zone will be common for the

components and will be designated $LZ_n...R2/R1$ etc. For the combination sample and Reactant*, the application zone will be $LZ_n.R*/S$ ($n' = n''$). That liquid_n is intended for transport of a certain reactant includes that the reactant in question also can be predeposited in the zone LZ_n . The latter includes that the reactant may be predeposited in an area downstream of the application zone for the relevant liquid but upstream of the nearest downstream located LZ (LZ_{n-1}), or if $n = 1$ only upstream of the detection zone (as LZ_{n-1} then is lacking).

By predeposition is meant that a reactant is added in advance to the matrix and in a way so as not to spread in the matrix until it is reached by liquid, which has been applied to initiate flow. Predeposition of reactants may be performed in a way known per se. (See e.g. Behringwerke US 4,861,711; Unilever WO 88/08534; Abbot US 5,120,643; Becton Dickinson EP 284,232). It is important that arrangements are made so that the reactant in question is quickly dissolved, when liquid passes through an area, containing predeposited reactant. In order to achieve quick dissolution it has been common to incorporate reactants in substances that as such dissolve quickly. This type of substances are often hydrophilic with polar and/or charged groups, such as hydroxy, carboxy, amino, sulphonate etc. In particular there may be mentioned hydrophilic quickly soluble polymers, e.g. having carbohydrate structure, simple sugars including mono-, di- and oligosaccharides and corresponding sugar alcohols (mannitol, sorbitol etc.). It is common practice to first coat the application zone in question with a layer of the quickly soluble substance, and then the reactant is applied, optionally followed by one additional layer of quickly soluble substance. An alternative way is by incorporating the reactant in particles of quickly soluble material which then are deposited in the relevant zone of the matrix.

Some of the most important embodiments regarding the application zones for liquid may be summarized: $2 \leq m \leq 6$; n' is 1, 2 or 3; $n'' > n'$ or $n'' = n'$; $LZ_{n,S}$ is the application zone for sample and optionally also for

- 5 Reactant* or other reactant; $LZ_{n'+1}$, $LZ_{n'+2}$, $LZ_{n'+3}$, $LZ_{n'-1}$, and $LZ_{n'-2}$ are application zones for liquids intended for transport of Reactant* or other reactant or buffer without reactant as far as allowed by m , n'' and n' .
- 10 Transport flow through the particular types of matrix may be achieved by the action of capillary forces, e.g. by starting with a substantially dry matrix. A sucking body may be placed at the end of the flow as an aid. Flow, meaning transport of primarily only dissolved components,
- 15 may be achieved if an electrical field is applied across the matrix.

Test protocols

- By use of the invention reactants and analyte can be made
- 20 to migrate zonewise as individual components or together in different combinations towards the detection zone. The exact sequence of application zones is determined by the test protocol to be utilized.
- 25 The invention may be applied to competitive (inhibition) as well as non-competitive (non-inhibition) test variants irrespective of if these are simultaneous or sequential regarding any reactant. Illustrative systems are shown schematically below in form of the complexes formed. "-"
- 30 relates to firm anchoring to the matrix, "---" relates to binding via biospecific affinity. For the sake of simplicity it has been assumed that reactants used are monovalent regarding utilized binding sites.

A. Sandwich protocol (non-inhibition)

Reactant I and Reactant* both have biospecific affinity for the analyte. x = number of moles of Reactant I on the matrix and y = number of moles of analyte (= number of moles of Reactant*), bound to Reactant I.

Complex in the detection zone:

Matrix (-Reactant I) _{x} (-Reactant I --- analyte --- Reactant*) _{y}

10

Simultaneous variants:

$m = 2$: LZ₂R*/S LZ₁B DZ

Sequential variants:

15 $m = 2$: LZ₂R* LZ₁S DZ.

$m = 3$: LZ₃R* LZ₂B LZ₁S DZ and alternatives where the buffer zone has position 1 or 3.

$m = 4$: LZ₄B LZ₃R* LZ₂B LZ₁S DZ and alternatives where any of the buffer zones is placed in position 1.

20 $m = 5$: The same sequence as for $m = 4$ with the exception that an extra buffer zone is placed in position 1.

B. Sandwich protocol (non-inhibition):

Reactant I exhibits biospecific affinity for Reactant II.
25 Both Reactant II and Reactant* have biospecific affinity for the analyte. x = number of moles of Reactant I on the matrix, y = number of moles of analyte (= number of moles of Reactant*), bound to Reactant I via Reactant II. $y + z$ is the number of moles of Reactant II bound to Reactant I.

30

Complex in the detection zone:

Matrix (-Reactant I) _{x} (-Reactant I --- Reactant II) _{z} (-Reactant I --- Reactant II --- analyte --- Reactant*) _{y}

35 Simultaneous variants:

$m = 2$: The same as for protocol A with the exception that LZ₂R*/S is LZ₂R*/S/RII or that LZ₁B is LZ₁RII.

$m = 3$: LZ₃R*/S LZ₂B LZ₁RII DZ or

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m = 2: The same as for protocol A with the exception that
5 LZ,S is replaced by LZ,S/RII.

m = 4, 5, 6: In analogy with protocol A sequences with up
10 to 6 application zones for liquid may be considered.

Reactant I is an analyte analogue, firmly anchored to the matrix, Reactant III exhibits biospecific affinity for the analyte and Reactant* has biospecific affinity for Reactant III. x = number of moles of Reactant I on the matrix. y = number of moles of Reactant III (= number of moles of Reactant*), bound to the matrix via Reactant I. The conditions are selected so that y is a measure of the amount of analyte in the sample.

Matrix $(-\text{Reactant I})_{x-y} \quad (-\text{Reactant I} \text{ --- Reactant III --- Reactant*})_y$

$$m = 2: \quad \text{LZ, R}^*/\text{RIII/S} \quad \text{LZ, B} \quad \text{DZ.}$$

30 m = 2: LZ₂R* LZ₁/RIII/S DZ.

$m = 3, 4$ and 5 : May be built up in analogy with protocol A.

Reactant I exhibits biospecific affinity for both Analyte
35 and Reactant*. Reactant* is a soluble analyte analogue. $x + y$ is the number of moles of Reactant I on the matrix, x and y are the number of moles of Reactant* and Analyte, respectively, being bound to the matrix.

Complex in the detection zone:

Matrix (-Reactant I --- Reactant*)_x (-Reactant I ---
Analyte)_y:

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Simultaneous variant:

m = 2: LZ₂R*/S LZ₁B DZ

Sequential variant:

10 m = 2: LZ₂R* LZ₁S DZ

m = 3, 4 and 5 may be built up in analogy with protocol A.

Matrices

The matrix defines the space in which the flow is
15 transported. The matrix may be the inner surface of a
simple flow channel (e.g. a capillary), the inner surface
of a porous matrix having a system of flow channels (porous
matrix) etc. extending through. For the sake of simplicity,
matrices, usable in this variant of the invention, will be
20 called flow matrices. Porous matrices may exist in the form
of monoliths, sheets, columns, membranes, single flow
channels having capillary dimensions or aggregated systems
of such flow channels etc. They may also exist in the form
of particles packed in column casings, compressed fibres
25 etc. The inner surface of the matrices, i.e. the surface of
the flow channels, should be hydrophilic, such that aqueous
media (usually water) may be absorbed and transported
through the matrices. The smallest inner dimension of the
flow channels should be sufficiently large for allowing
30 transport through the matrix of the reactants being used.
The rule of thumb is that suitable matrices are selected
among those having flow channels with the smallest inner
dimension (often as a diameter for round channels) in the
interval 0.4-1000 µm, preferably 0.4-100 µm if the matrix
35 exhibits a system of mutually communicating flow channels.
Flow channels having a smallest inner dimension in the
upper part of the interval 0.4-1000 µm are primarily of

Discussion The purpose of this study was to determine the effect of the use of a mobile phone on the performance of a concurrent task. The results of this study indicate that the use of a mobile phone significantly affected the performance of a concurrent task. The use of a mobile phone significantly increased the time taken to complete the task, and significantly decreased the accuracy of the task. The use of a mobile phone also significantly increased the number of errors made during the task. The results of this study indicate that the use of a mobile phone significantly affected the performance of a concurrent task. The use of a mobile phone significantly increased the time taken to complete the task, and significantly decreased the accuracy of the task. The use of a mobile phone also significantly increased the number of errors made during the task.

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Detection zone

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5 Hybritech EP 437,287 and EP 200,381; Grace & Co. EP 420,053; Fuji Photo Film US 4,657,739; Boehringer Mannheim WO 94/06012. For the invention the latter variant with smaller particles adsorbing physically to the matrix has been shown to be good.

In one and the same transport flow there may be several detection zones (DZ1, DZ2 etc.). One or more of the detection zones may relate to the same or different analytes. If the analytes are different Reactant I is usually different for each DZ.

[illegible]

30 A preferred label group is particles optionally containing any of the detectable groups above, such as fluorophoric groups or chromogenic groups (coloured particles). Useful particles often have a size in the interval of 0.001-5 μm . The particles may have colloidal dimensions, so called sol
35 (i.e. usually spherical and monodisperse having a size in the interval 0.001-1 μm). Especially metal particles (e.g. gold sol), non-metal particles (e.g. SiO_2 , carbon, latex

and killed erythrocytes and bacteria) may be mentioned. Also particles of non-colloidal dimensions but with focus on non-sedimenting capability have been used. These have been more or less irregular and more or less polydisperse
5 (carbon particles < 1 μm ; Pharmacia AB, WO 96/22532).

For particles as label group reference is made to Unilever WO 88/08534; Abbott US 5,120,643; Becton Dickinson EP 284,232 among others.

10

In connection with the development that has led to the present invention it was surprisingly found that good results may be obtained if one simultaneously utilizes:

- 15 (a) Reactant* with label particles according to the above as a detectable group, and
- (b) a detection zone, in which Reactant I has been anchored to the matrix via particles substantially
20 having dimensions that would allow transport of the particles as such through the matrix.

We have achieved functioning systems, in which label particles and anchoring particles substantially have the
25 same dimensions. This means with great probability that the label particles may be larger than the anchoring particles and vice versa, as long as they remain smaller than the flow channels defined by the matrix. The system may function with or without pre-deposition of Reactant* in the
30 intended application zone. This embodiment is part of an invention, described in our co-pending PCT application: "Analytical method using particles and test kit for performing the method" (based on SE 9704935-7). This separate patent application is incorporated herein by
35 reference.

Analytes

The invention is primarily adapted for determination of biospecific affinity reactants of the types initially mentioned. The reactants may be a cell or a virus or a part thereof. In particular antigen, such as an immunoglobulin or an antibody may be mentioned. For immunoglobulins the determination may relate to a certain Ig and/or certain Ig subclass. For antibodies the determination may relate to a certain specificity, optionally also the Ig class or the Ig subclass of the antibody. Relevant Ig classes are IgA, IgD, IgE, IgG and IgM. Relevant Ig subclasses are IgG1, IgG2, IgG3 and IgG4.

In sandwich variants (according to protocols A and B, above) the analyte may be an antibody, directed to an allergen/antigen/hapten and be derived from a certain species, a certain Ig class or a certain Ig subclass. In this case Reactant* may be an analytically detectable antibody directed to an epitope specific for the species, Ig class or Ig subclass and with Reactant I (protocol A) or Reactant II (protocol B) as the allergen/antigen/hapten. Alternatively the reverse may be selected, i.e. Reactant* is the allergen/antigen/hapten and Reactant I and Reactant II, respectively, is the antibody, directed to the analyte. When the analyte is an antigen in general, both Reactant I and Reactant* may be antibodies, directed to the antigen, in protocol A. For protocol B it is Reactant II and Reactant* that are antibodies directed to the antigen.

Competitive variants are most interesting for low molecular analytes. Illustrative examples are antigen and hapten. For protocol C Reactant I may be the antigen or the hapten, firmly anchored to the matrix, Reactant III may be an antibody, directed to the antigen, and Reactant* may be an antibody, directed to Reactant III. For protocol D Reactant I may be an antibody directed to the analyte and Reactant* may be the analyte labelled with an analytically detectable group.

The method of the invention may be performed as part of diagnosing allergy or autoimmune disease.

- 5 For the inventors it has been of special interest to measure anti-allergen antibodies of IgE or IgG class, for the latter preferably with focus on any of the subclasses mentioned. Measuring of allergen-specific antibodies can be utilized when diagnosing IgE mediated allergy.

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Samples

- Relevant samples may be of biological origin, e.g. from different body fluids (whole blood, serum, plasma, urine, saliva, tear fluid, cerebrospinal fluid etc.), from cell
15 culture media, processing procedures in biotechnology, from tissue extracts, from food stuff, from the environment (environmental analysis samples) etc. The samples may be pretreated in order to fit e.g. the matrix, the test protocol involved etc.

20

Calibrators

- Determination methods of the type that the invention is related to, involve that the detectable signal from the analytically detectable reactant (Reactant*) is measured
25 and the measured signal (sample value) is taken as a measure of the amount of analyte present in the sample. To transfer the measurement signal to actual amounts of analyte the signal is usually compared to the corresponding signal (calibrator value) of known standard amounts of
30 analyte (calibrators). In connection with the present invention a new calibrator system has been developed, which applied to the present invention constitutes a best embodiment.

- 35 This separate invention means that the used calibrator in advance has been anchored to a matrix (matrix calibrator), preferably of the same type as the one utilized for sample run. When measuring calibrator values, matrix calibrator is

allowed to bind to Reactant*, and then the measurement signal from Reactant* is measured in a way known per se. By utilizing different amounts of matrix calibrator a series of calibrator values may be obtained corresponding to
5 different pre-determined amounts of analyte in sample (standard amounts, dose-response curve, calibration curve).

Alternatively, instead a binder for the calibrator has been anchored to the matrix, and calibrator is added at the
10 determination of calibrator value, optionally pre-deposited in the matrix upstream of the calibrator zone(s) to be dissolved by sample solution or buffer at the determination. When a calibrator binder is bound to the matrix, the calibrator may either be movably (diffusively)
15 pre-deposited in the matrix in a zone separated from the detection zone, or be added together with or separately from the sample. The calibrator binder is usually one member of a specific binding pair (reactant pair), the other member of the binding pair being coupled or
20 conjugated to the calibrator substance. As examples of such specific binding pairs may be mentioned immunological binding pairs such as antigen-antibody and hapten-antibody, biotin-avidin or -streptavidin, lectin-sugar, hormone-hormone receptor, nucleic acid duplex.

25 Applied to the present invention our new calibrator system involves primarily that the transport flow passes one or more zones with a calibrator, firmly anchored to the matrix in the respective calibrator zone (CZ).

30 Anchoring of a calibrator to the matrix in a calibrator zone may be performed according to the same principles as for anchoring of Reactant I to a detection zone.

35 Calibrator zones should be located downstream of an application zone for liquid, intended for transport of Reactant*. In relation to the detection zone (DZ) the calibrator zone is preferably located upstream.

Our invention relating to calibrators is described in detail in our co-pending PCT application with the title "Method using a new calibrator and a device and test kit including the calibrator" (based on SE 9704933-2). This application is incorporated herein by reference.

A second main aspect of the invention

The flow matrix according to the above containing two or more application zones for liquid, optionally in the form of a kit wherein the flow matrix is comprised together with the analytically indicatable reactant, constitutes a second main aspect of the invention.

The invention is illustrated in the following non-limiting experimental part.

EXAMPLE 1: SEQUENTIAL METHOD WITH THE ZONE SEQUENCE: LZ₄B, LZ₃R*, LZ₂B, LZ₁S, DZ. DETECTION OF hIgE IN TEST VARIANT WITH CARBON PARTICLE CONJUGATE

Methods and materials

Adsorption of phenyldextran to polystyrene particles:

Phenyldextran (substitution degree: 1 phenyl group on each fifth monosaccharide unit = 20%, Mw dextran 40,000, Pharmacia Biotech AB, Uppsala, Sweden) was adsorbed to polystyrene particles (0.49 µm Bangs Laboratories, USA) by incubations under stirring with phenyldextran dissolved in deionized water to 1) 5 mg/ml, 10% particle suspension, RT 30-60 minutes; 2) 5 mg/ml, 5% particle suspension, RT 1 h; 3) 20 mg/ml, 1-2% particle suspension, RT 3 h or overnight. The particles were subsequently washed twice with deionized water. The particle suspensions were centrifuged between each incubation and wash (12,100xg, 25 min, Beckman, J-21, JA-20, 10,000 rpm). The particle suspension was finally sonicated (Ultrasonic bath, Branson 5210, 5 min).

Coupling of anti-human IgE antibody (anti-hIgE) to polystyrene particle: Anti-hIgE was coupled to phenyldextran coated polystyrene particles with CDAP (1-cyano-4-dimethylamino-pyridinium bromide (Kohn J and
5 Wilchek M, FEBS Letters 154(1) (1983) 209-210).

Desalting and change of buffer of anti-hIgE was performed by gel filtration (PD-10, Pharmacia Biotech AB) in NaHCO_3 , 0.1 M, pH 8.5. 2.3 g of polystyrene particles (coated with
10 phenyldextran according to above) in 2% solution in 30% (by volume) acetone were activated with 17 ml CDAP (0.44 M) and 14 ml TEA (0.2 M triethylamine, Riedel-deHaën, Germany). CDAP was added with stirring for 150 seconds and TEA for 150 seconds. The particles were washed with 30% (by volume)
15 acetone and centrifuged at 12,100xg (25 min, Beckman, J-21, JA-20, 10,000 rpm). 17 of anti-hIgE was coupled to the activated particles (2%, 0.15 g in 0.1 M NaHCO_3 , pH 8.5) in incubating with stirring overnight at +4°C. The particles were centrifuged and decanted before deactivating with
20 glutamic acid 0.05 M and aspartic acid 0.05 M in 0.1 M NaCHO_3 , pH 8.5 when incubating with stirring overnight at +4°C. Coupled particles were washed once with 0.1 M NaHCO_3 , 0.3 M NaCl, pH 8.5, once with 0.1 M HAc, 0.3 M NaCl pH 5, once with 0.1 M NaHCO_3 , pH 8.5 and once with 20 mM borate
25 buffer pH 8.5.

The concentration of particles was determined spectrophotometrically at A_{600} nm with untreated particles as reference. Concentration of coupled protein was
30 determined by having anti-hIgE present during the coupling and cpm measurement.

Carbon particle conjugate (Reactant*): This was prepared by anti-hIgE being adsorbed to carbon particles (sp100, < 1
35 μm , Degussa, Germany) according to WO 96/22532 (Pharmacia AB). The final solution used in the flow matrix contained 400 μg of carbon particles per ml.

Deposition of anti-hIgE-coupled particles on membrane: On nitrocellulose sheets (Whatman, 8. μ m, length 5 cm and width 25 cm with polyester backing, anti-hIgE particles (prepared according to the above) were deposited in a zone over the width of the sheet (future detection zone) with Linear Striper (IVEK Corporation). The flow was 1 μ l/sec and 1 μ l/cm. The particles were diluted in borate buffer (20 mM, pH 8.5, Dextran T5000 4.2% w/w, sorbitol 5.8% w/w). The amount of deposited anti-IgE antibody was about 1000 ng/cm. The sheets were dried for 1 h at 30°C.

Zones for application of buffer, sample and carbon particle conjugate: Well separated from the zone, containing deposited material, 4 Inplastor strips (Mylar with glue on one side, Gelman) with a width of 1 mm were placed in parallel with the zone and parallel with each other at a distance of 5 mm from each other (zone spacers). The Inplastor strips thus defined four zones with a width of 5 mm. The sheets were cut perpendicularly relative to the zone containing deposited material, to strips with a width of 0.5 cm (the length of the strip then became 5 cm) (Singulator: Matrix 1201 membrane cutter, Kinematic automation). The final strips exhibited four parallel zones (application zones) separated by Inplastor strips as zone spacers and a separate zone with deposited anti-hIgE antibody (detection zone). As a comparison strips without zone spacers, i.e. without separated application zones were produced.

Test methodology: Strips with separated application zones were mounted on a plane holder. At the top (0.5 cm) of the strip (and with the detection zone as the nearest zone) a sucking membrane was placed (Whatman, 17 Chr, width 3 cm). The holder also gave a constant pressure on the sucking membranes. For simultaneous application of reagents to the four subzones a 4 channel Multipipette (Labsystems) was

used. The multipipette was loaded so that serum sample (30 μ l) was applied in the application zone nearest to the detection zone in the order of buffer (30 μ l), carbon particle conjugate (30 μ l) and buffer (30+30 μ l) in the
5 respective upstream application zone. For sequential application to the strips without zone spacers, 30 μ l of sample were first applied to the lower end of the strip. After suction of sample volume, buffer (30 μ l), carbon particle conjugate (30 μ l) and buffer (30+30 μ l) were added
10 successively after suction. The carbon particle conjugate was prepared according to above and suspended in buffer. The buffer was NaPO_4 0.1 M, BSA 3%, NaN_3 0.05%, sucrose 3%, sodium chloride 0.2%, phenyldextran 0.05%, bovine gammaglobulin 0.05%, pH 7.5. The binding of the carbon
15 particle conjugate to the detection zone was quantitated by measuring of absorbance (Ultroscan XL, Enhanced Laser Densitometer, LKB). IgE with standard concentrations in plasma environment (0; 0.5; 2; 10; 50, and 200 KU/L) was used as samples.

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Results

Having four application zones for liquid and simultaneous addition, the liquids were migrating in the order of the application zones, i.e. the sample being in the zone
25 nearest to the detection zone was migrating first, without being mixed with the washing solution of the following application zone, which solution in turn started migrating, when the sample had been transported out of the application zone for samples. Correspondingly the liquids of the
30 remaining zones were migrating sequentially without being mixed.

Table 1: Analysis results from runs with sequential addition in one zone and from simultaneous addition in four
35 subzones (buffer, analytically detectable reactant, buffer, sample).

IgE KU/L	Sequential addition in one zone (Abs x1000)	Simultaneous addition in 4 subzones (Abs x1000)
0,5	0	12
2	312	207
10	1241	831
50	1921	1560
200	2115	2044

In Table 1 is shown that the uptake decreases slightly for strips with discrete application zones compared to when addition is performed in one and the same zone. The decrease is, however, marginal. Therefore the experiment shows that generally the same result may be achieved if simultaneous addition is performed to the zone sequence LZ₄B, LZ₃R*, LZ₂B, LZ₁S as if sample, Reactant* and buffer are added sequentially to a common application zone.

If a firmly anchored anti-IgE antibody (Reactant I) is replaced by an allergen a determination method for IgE antibodies directed to the allergen is obtained. Analogously, test systems related to antibodies of another class/subclass and with another specificity may be determined. Application zones for only buffer may be omitted. For additional alternative test protocols and analytes see above under the headings "Test protocols" and "Analytes".

EXAMPLE 2: SEQUENTIAL METHOD WITH THE ZONE SEQUENCE: LZ₄B, LZ₃R*, LZ₂B, LZ₁S, DZ. DETECTION OF hIgE IN TEST VARIANT WITH FLUORESCENT DETECTION CONJUGATE

5 Methods and materials

Coupling of anti-human IgE antibody (anti-hIgE) to a polystyrene particle: Anti-hIgE was coupled to polystyrene particles coated with phenyldextran (prepared according to Example 1) with CDAP (1-cyano-4-dimethylaminopyridinium bromide) (Kohn J and Wilchek M, FEBS Letters 154(1) (1983) 209-210). Desalting and buffer change of anti-hIgE was performed by gel filtration (PD-10, Amersham Pharmacia Biotech AB) in NaHCO₃, 0.1 M, pH 8.5.

15 0.35 g of polystyrene particles (2% solution) were activated with 5.2 ml of CDAP (0.44 M) and 4.2 ml of TEA (0.2 M triethylamine, Riedel-deHaën, Germany). CDAP was added with stirring for 60 seconds and TEA for 120 seconds. A five times excess of ice-cooled deionised water was
20 added. The particles were centrifuged at 12,100xg (25 min., Beckman, J-21, JA-20, 10,1000 rpm). The resulting pellet was dissolved in ice-cooled, deionized water and washed once with ice-cooled deionized water and then centrifuged at 12,000 x g. 50 mg of anti-hIgE were coupled to the
25 activated particles (2%, 0.35 g in 0.1 M NaHCO₃, pH 8.5). Incubation with stirring was the performed for 1 hour at +4°C. After centrifugation, the particles were deactivated with glutamic acid, 0.05 M, and aspartic acid, 0.05 M in 0.1 M NaHCO₃, pH 8.5. Incubation and stirring was then
30 performed overnight at +4°C. Coupled particles were washed twice with 20 mM borate buffer, pH 8.5, whereupon the particle concentration was determined spectrophotometrically at A_{600nm} with untreated particles as reference. Coupled protein concentration was determined
35 by having radioactive anti-hIgE present during the coupling.

Coupling of anti-hIgE antibodies to detection particles:

Antibodies to hIgE cleaved with pepsin to fab'2 fragments were coupled to fluorescent polystyrene particles having aldehyde groups on their surface (Molecular Probes C-17177

5 TransFluoSphere, aldehyde-sulphate microspheres, 0.1 μ m, 633/720, 2% solids). 23 mg of antibody were then coupled to 66 mg of particles in 50 mM NaPO₄, pH 6.5, overnight at room temperature, whereupon 205 μ L of NaCNBH₄ (5 M) were added to reduce the coupling for 3 hours at room

10 temperature. Centrifugation was performed at 20,800 x g for 50 minutes (50 minutes in Eppendorf 5417R, 14,000 rpm), and deactivation in glutamic acid, 0.05 M, and aspartic acid, 0.05 M, in deionized water, pH 6.5, was then performed overnight with stirring at room temperature. After

15 centrifugation again at 20,800 x g, blocking was performed with 0.2% BSA in 50 mM NaPO₄, pH 7.4, with 0.05% NaN₃ and incubation was carried out overnight at +4°C.

Centrifugation was then performed again at 20,800 x g and washing was performed twice with blocking buffer which was then used also for storage. The particle concentration was determined in a fluorimeter (Perkin-Elmer LS50B) with a standard curve prepared with the original particle. Coupled protein concentration was determined by having radioactive hIgE present during the coupling.

25

Deposition of anti-hIgE-coupled particles on membrane and application zones:

Was performed according to Example 1, except that the Inplastor strips were replaced by strips of adhesive tape (2 mils clear polyester Arcare with glue on one side).

30

Test methodology: Strips with spaced application zones were mounted to an inclined plane, about 16°, in a holder. At the top (0.5 cm) of the strip (and with the detection zone as the nearest zone), two sucking membranes (Whatman, 17

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Chr, width 3.4 cm) were placed on top of each other. The holder also exerted a constant pressure on the sucking

membranes. For simultaneous application of reagents to the four subzones, a multichannel Finn pipette (Labsystems) was used. The multipipette was charged so that serum sample (30 μ L) was applied to the application zone nearest to the

5 detection zone in the order of buffer (15 μ L), fluorescent particle conjugate (30 μ L) and buffer (30 + 30 μ L) in the respective application zone located upstream. For sequential application to the strips without zone spacer, 30 μ L of sample were first applied to the lower end of the

10 strip. After sucking of the sample volume, buffer (15 μ L), detection particle conjugate (30 μ L) and buffer (30 + 30 μ L) were successively added after sucking. The particle conjugate was suspended in assay buffer consisting of NaPO_4 0.1 M, BSA 3 %, NaN_3 0.05 %, sucrose 10 %, NaCl, 0.15 M,

15 bovine gammaglobulin 0.05 %, pH 7.5. The measurement of time started with the application of the sample, and the time until the last buffer had been sucked into the membrane was noted. The binding of the fluorescent particle conjugate to the detection zone was quantified by scanning

20 with a red diode laser (635 ± 5 nm). As sample were used IgE standard concentrations in plasma environment (0, 0.5, 2, 10, 50 and 200 KU/L).

Results:

25 Precisely as in Example 1, the liquids migrated out of the application zone in the existing order. The time for a whole test with simultaneous application was about 20 minutes, and the time for a test with sequential

30 application was about 25 minutes.

Table 2: Analysis results from runs with sequential application in one zone and from simultaneous application in four subzones (buffer, analytically detectable reactant, buffer, sample).

KU/L	Simultaneous addition to four subzones	Sequential addition to one zone
0	0.048*	0.038*
0.5	0.053	0.047
2	0.085	0.074
10	0.286	0.256
50	1.334	1.291
200	2.507	2.487

* = scanning signal (Vmm)

Table 2 shows that the uptake is comparable for strips with discrete application zones in comparison with addition to a single zone. The experiment therefore shows that the same result may be obtained if addition is made simultaneously to the zone sequence LZ₄B, LZ₃R*, LZ₂B, LZ₁S as if sample, Reactant* and buffer are added sequentially to a common application zone.

EXAMPLE 3: SEQUENTIAL METHOD WITH THE ZONE SEQUENCE: LZ₅B, LZ₄R*, LZ₃B, LZ₂S, LZ₁B, DZ. DETECTION OF BIRCH-SPECIFIC hIgE IN TEST VARIANT WITH FLUORESCENT DETECTION CONJUGATE

Methods and materials

Extraction of birch pollen allergen t3, Betula verucosa: 1 part (weight) of birch pollen (Allergon, Sweden) was extracted with 10 parts (volume) of 0.1 M phosphate buffer, pH 7.4. The extraction was continued for 2 hours on a shaker table at +4 °C. The extract was centrifuged at 4000 rpm for 1.75 hours. After filtration, the solution was applied to a PD-10 column (Pharmacia Biotech AB) and eluted in 0.1 M NaHCO₃, pH 8.5. The t3 eluate (designated: t3 extract 1/14) was taken to amino acid analysis for determination of the total protein content.

Coupling of birch pollen allergen to polystyrene particle:
t3 extract was coupled to phenyldextran coated polystyrene particles (prepared according to Example 1) with CDAP. The coupling was effected analogously with the coupling of
5 hIgE.

Polystyrene particles (2128 mg) coated with phenyldextran in 30 % (by volume) acetone, 2 % particle suspension, were activated with 954 mg of CDAP (100 mg/ml in 30 % acetone)
10 and 7.63 ml of 0.2 M triethylamine (TEA, Riedel-de Haen, Germany). CDAP was added with stirring and TEA was added dropwise for 90 seconds and with stirring for totally 120 seconds. The reaction was stopped by the addition of 30 % acetone (4 times the volume) and centrifugation at 12,400 g
15 for 35 minutes. The particles were washed once with deionized water.

640 ml of t3 extract 1/14 in 0.1 M NaHCO_3 , pH 8.5, were added to the activated particles, and coupling was
20 continued for 1 hour on a shaker table. After centrifugation, the particles were deactivated with 0.05 M aspartic acid and 0.05 M glutamic acid in 0.1 M NaHCO_3 , pH 8.5. Incubation then took place on a shaker table overnight at +4 °C. The particles were then washed twice with 50 mM
25 NaPO_4 , 0.05 % NaN_3 , pH 7.4. The particle concentration was determined spectrophotometrically at 600 nm with uncoated polystyrene particles as reference. t3-coupled polystyrene particles were taken to amino acid analysis for determination of the total protein content.

30

Deposition of t3-coupled polystyrene particles on a membrane: To nitrocellulose sheets with polyester backing (Whatman, 8 μm , 5 cm width) were applied zones of t3-coupled particles diluted to 4 % particle content in 50 mM
35 NaPO_4 , 10 % sucrose, 0.05 NaN_3 , pH 7.4. The deposits were dried for 1 hour at 30 °C.

Zones for application of buffer, sample and detection particle conjugate: Five 1 mm wide strips of adhesive tape (2 mils clear polyester, Arcare with glue on one side) were placed well separated from the zone containing the deposited material and in parallel with the zone at a distance of 5 mm from each other. The tape strips thereby defined five different 5 mm wide zones. The sheets were cut perpendicularly to the zone containing deposited material to strips having a width of 0.5 cm (the length of the strip then became 5 cm) (Singulator: Matrix 1201 membrane cutter, Kinematic automation). The final strips exhibited five zones (application zones) separated by tape strips as zone spacers and a separate zone with deposited birch pollen (detection zone). Strips without zone spacers, i.e. without separated application zones, were prepared as a comparison.

Test methodology: Strips with separated application zones were mounted, and reagents were applied as in Example 2. Buffer (20 μ L) was applied to the zone closest to the application zone, and then serum sample (30 μ L), buffer (20 μ L), detection particle conjugate (20 μ L) and buffer (30 + 30 μ L) in the respective application zone located upstream. For sequential application to the strips without zone spacer 20 μ L of buffer were first applied to the lower end of the strip, and after sucking in thereof, 30 μ L of sample were applied in the same position and then buffer (20 μ L), fluorescent particle conjugate (20 μ L) and buffer (30 + 30 μ L). Before all applications, the preceding application had been sucked in by the strip. The detection particle conjugate and the buffer were according to Example 2.

Results:

With the application zone consisting of five subzones and with simultaneous addition thereto, it turned out that the liquids, precisely as in the Examples above, migrated out of the application zone in the existing order. The time

required for a whole test with simultaneous addition was about 21 minutes, and the time needed for a whole test with sequential addition was about 27 minutes.

- 5 **Table 3:** Analysis results from runs with sequential addition in one zone and from simultaneous addition in 4 subzones (buffer, analytically detectable reactant, buffer, sample).

	Simultaneous addition to 5 subzones	Sequential addition to 1 zone
neg	0.067*	0.058*
pos 1	1.911	2.608
pos 2	0.299	0.375

10 * = scanning signal (Vmm)

Table 3 shows that the uptake is decreased to some extent for strips having discrete application zones compared with
15 addition to a single zone. The decrease is, however, marginal and is probably due to the fact that the flow rate in simultaneous application was somewhat delayed. The experiment therefore demonstrates that basically the same results may be achieved for simultaneous application to the
20 zone sequence LZ₅B, LZ₄R*, LZ₃B, LZ₂S, LZ₁B as if sample, Reactant* and buffer are applied sequentially to a common application zone.